A WEARABLE ELECTRONIC MONITORING DEVICE FOR LOW PRESSURE GARMENT APPLICATIONS AND TEMPERATURE ANALYSIS FOR PREVENTION OF

ULCERATION AND INFECTION

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ABSTRACT

The healing process of several medical conditions related to venous insufficiency and burn scar management can be improved by the proper application of pressure. Current practices for applying pressure to an extremity do not guarantee the consensus ideal interface pressures for such medical conditions. Applying a low pressure range (within 15 - 40 mm Hg) is challenging due to many factors, but especially because the actual pressure applied by a compression garment used on a patient is unknown. The proposed device, used to sense and display low pressure values, is described in detail throughout the chapters of this thesis.

An electronic device was designed, fabricated, assembled, calibrated, and tested in order to deliver a small wearable electronic system which can measure and provide low pressure values inside the range of interest. The sensing unit is intended to be placed underneath the compression garment against the arm or leg of the subject and take force (which is then converted to pressure) and temperature readings. These readings are analyzed by the microcontroller and sent via Bluetooth to the smart phone application where they can be reviewed by the user to make appropriate adjustments to the applied pressure, if necessary. The purpose of the thermal sensor is to sample the skin temperature over a period of time and use the collected data to determine the potential presence of skin infections. The four major elements that complete this system are the sensor unit, the controlling unit, the Bluetooth module, and the smart phone application, which can be powered by a single 3.7V rechargeable battery lasting tens of hours without replacement. The system can be adapted to run for several days if timers are implemented. The test results conducted to the wearable gadget show exceptional linearity and accuracy within 1N range (75 mm Hg), providing a promising solution for sensing low pressure values.

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ABSTRACTiii
ACKNOWLEDGEMENTS iv
TABLE OF CONTENTS vi
LIST OF TABLES
LIST OF FIGURES ix
CHAPTER 1: INTRODUCTION 1
1.1 BACKGROUND 1
1.2 PROBLEMS WITH CURRENT COMPRESSION METHODS
1.3 PROPOSED METHOD AND OBJECTIVES
CHAPTER 2: DESIGN OF ELECTRONIC MONITORING DEVICE
2.1 DESIGN OVERVIEW
2.1.1 PRINCIPLE OF OPERATION
2.2 THE SENSOR UNIT 10
2.2.1 FORCE SENSOR 11
2.2.2 TEMPERATURE SENSOR 14
2.2.3 PCB DESIGN OF SENSOR UNIT 15
2.2.4 SPRING-LOADED PINS (POGO PINS) 17
2.2.5 SENSOR UNIT ASSEMBLY 18
2.3 CONTROLLING UNIT
2.3.1 PIC18 MICROCONTROLLER
2.3.2 THE INSTRUMENTATION AMPLIFIER
2.3.3 BUCK-BOOST CONVERTER

2.4 BLUETOOTH LOW ENERGY (BLE) MODULE	30
2.4.1 BLUTOOTH PRINCIPLE OF OPERATION	30
2.4.2 BLUETOOTH HM-10 MODULE	
2.5 DESIGN OF SMART PHONE APPLICATION	33
2.5.1 WEB-BASED APPLICATION IDE	
2.5.2 COMPOSITION OF MOBILE PHONE APPLICATION STRUCTURE	
CHAPTER 3: FLOW OF DATA AND COMMUNICATION	
3.1 MPLAB X IDE SOFTWARE AND PROGRAMMER	
3.2 MPLAB C CODE	39
3.2.1 THE SENSING STAGE	40
3.2.2 DATA PROCESSING AND DATA LABELING STAGE	43
3.2.3 DATA ARRANGEMENT STAGE	50
3.3 MIT APP INVENTOR CODE	52
CHAPTER 4: PROTOTYPE AND PERFORMANCE RESULTS	58
4.1 PROTOTYPE AND DEVICE COST BREAKDOWN	58
4.2 PROTOYPE PERFORMANCE TEST RESULTS	61
CHAPTER 5: CONCLUSION AND FUTURE WORK	67
5.1 CONCLUSION	67
5.2 FUTURE WORK	68
APPENDIX I: COMPLETE MPLAB X C CODE	73
APPENDIX II: COMPLETE MIT APP INVENTOR BLOCK CODE	
REFERENCES	80
CURRICULUM VITAE	

LIST OF TABLES

Table 2.1	Power modes for CC2541 Bluetooth SoC
Table 2.2	Phone application functionality list
Table 4.1	Cost breakdown of sensor unit
Table 4.2	Cost breakdown of controlling unit with Bluetooth included 60

LIST OF FIGURES

Figure 1.1	Stages of chronic venous insufficiency (CVI) [10]
Figure 1.2	Keloid scar with finite element analysis (FEA) showing tension levels [16]
Figure 1.3	Patient pressure value reading over the course of several months [11]
Figure 1.4	Pressure ulcer due to improper stocking size [18]7
Figure 2.1	System design concept and flow of communication9
Figure 2.2	System sensor unit (Solidworks model) 11
Figure 2.3	a) Force sensor and b) its circuit diagram [20]
Figure 2.4	Wheatstone bridge circuit
Figure 2.5	Temperature sensor size and package [21] 15
Figure 2.6	Current and output voltage vs. ambient temperature [21] 15
Figure 2.7	Sensor unit top and bottom PCBs with schematics
Figure 2.8	Top and bottom 3D PCB models of sensor unit
Figure 2.9	Spring-loaded pin [22]18
Figure 2.10	Exploded view sensor unit assembly components
Figure 2.11	Sensor unit pressing and depressing operation
Figure 2.12	Plot of output voltage vs. mass
Figure 2.13	Plot of output voltage vs. force
Figure 2.14	Plot of output voltage vs. force with initial force removed
Figure 2.15	Temperature calibration setup of sensor unit
Figure 2.16	Plot of temperature chamber vs. temperature unit output voltage
Figure 2.17	Plot of IR thermometer and sensor unit temperature test
Figure 2.18	Temperature comparison of IR thermometer vs. unit senor after optimization 25

Figure 2.19	Main controlling unit schematic with Bluetooth included	26
Figure 2.20	Buck-boost efficiency plot	29
Figure 2.21	HM-10 Bluetooth module [27]	31
Figure 2.22	BLE pin configurator and typical connections [27]	32
Figure 2.23	Designer view window of MIT App Inventor	34
Figure 2.24	Smart phone application interacting with the system	36
Figure 3.1	MPLAB C code flowchart	10
Figure 3.2	Flowchart sensing stage portion	12
Figure 3.3	ADC conversions of force, temperature, and battery charge readings	13
Figure 3.4	Data processing and labeling stage	14
Figure 3.5	Obtaining voltage, force, and pressure values from their respective functions	15
Figure 3.6	Function to calculate the force from ADC readings	15
Figure 3.7	Function to calculate pressure (mm Hg) from the force values	16
Figure 3.8	Obtaining voltage and temperature values from their respective functions	17
Figure 3.9	Function that resets the ADC to take new analog input samples	17
Figure 3.10	Function that computes the temperature from the sensed signal	18
Figure 3.11	Computing battery voltage values from ADC readings	19
Figure 3.12	Formulation of data labels to be use by smart phone app	50
Figure 3.13	Organization of analyzed data prior to Bluetooth transmission	51
Figure 3.14	The combination of the data values and their assigned labels	51
Figure 3.15	Transferring data to the Bluetooth module	52
Figure 3.16	MIT App Inventor software windows: Blocks and Designer	53
Figure 3.17	Smart phone app flowchart	54

Figure 3.18	Removing unused characters from receiving data	55
Figure 3.19	Management of received data for proper label classification	56
Figure 3.20	Low voltage battery condition statement	56
Figure 3.21	Management of received data for appropriate storage options	57
Figure 4.1	Complete wearable device system	59
Figure 4.2	Force comparison test: wearable device vs. actual force with offset	53
Figure 4.3	Force comparison test: wearable device vs. actual force with no offset	53
Figure 4.4	Pressure comparison test: wearable device vs. calculated pressure with offset 6	54
Figure 4.5	Pressure comparison test: wearable device vs. calculated pressure with no offset 6	54
Figure 4.6	Temperature comparison test (1 st subject): wearable device vs. IR thermometer 6	55
Figure 4.7	Temperature comparison test (2 nd subject): wearable device vs. IR thermometer . 6	55
Figure 4.8	Battery life expectancy with one sensor	56
Figure 4.9	Battery life expectancy simulation with 10 sensors	56
Figure 5.1	Improved version of sensor unit	59
Figure 5.2	Low profile PCB connector	71
Figure 5.3	Comparison of BLE module sizes, HM-10 (left), HM-10 (middle), BM71 (right) 7	72
Figure A2.1	Smart phone app setup code	78
Figure A2.2	Smart phone data management code	79

REFERENCES

- [1] R. Weiss et al, "Venous insufficiency," USENET: drug and diseases.dermatology, Sep. 25, 2020 [Accessed Feb. 8, 2022].
- M. Porter, "A Case Study of Venous Leg Ulceration," in *British Journal of Community Nursing*, Aug. 2018. [Online]. Available: https://www.magonlinelibrary.com/doi/full/10.12968/bjcn.2018.23.Sup9.S30.
- [3] I. C. Valencia et al, "Chronic venous insufficiency and venous leg ulceration," *Journal of the American Academy of Dermatology*, vol. 44, no. 3, pp. 401-404, Mar. 2001.
 Available: ScienceDirect,

https://www.sciencedirect.com/science/article/pii/S0190962201031553#aep-section-id37.

- [4] C. V. Ruckley, "Socioeconomic impact of chronic venous insufficiency and leg ulcers."
 Sage Journals, vol. 48, no. 1, pp. 67-69, 1997.
- [5] "Chronic Venous Insufficiency," The John Hopkins University, Baltimore, Maryland, United States. Accessed: Feb. 8, 2022. [Online]. Available: https://www.hopkinsmedicine.org/health/conditions-and-diseases/chronic-venousinsufficiency.
- [6] B. Eklof et al, "Revision of the CEAP classification for chronic venous disorders: consensus statement," *Journal of Vascular Surgery*, vol. 40, no. 6, pp. 1248-1252, Dec. 2004. Available: ScienceDirect, https://www.sciencedirect.com/science/article/pii/S0741521404012777.
- [7] R. Weiss et al, "Venous insufficiency treatment & management," USENET: drug and disease.dermatology, Sep. 25, 2020. [Accessed Feb. 8, 2022].

- [8] J. Menezes, MD. (2021). Optimization of Compression Therapy Smart Stockings [PowerPoint slides].
- J. C. Mayberry et al, "Fifteen-year results of ambulatory compression therapy for chronic venous ulcers," Oregon Health Sciences University, Portland, Oregon, United States, PMID: 2020902, May 1, 1991. Accessed: Feb. 9, 2022. [Online]. Available: https://europepmc.org/article/med/2020902.
- [10] E. Conde, "CEAP Classification of Chronic Venous Disorders: Let's all speak about the same language," *elenaconde.com*, Jan. 20, 2019. [Online]. Available: https://www.elenaconde.com/en/ceap-classification-of-chronic-venous-disorders-lets-all-speak-the-same-language/. [Accessed Feb. 14, 2022].
- J. Wiseman et al, "Variability of pressure at the pressure garment-scar interface in children after burn: A pilot longitudinal cohort study," *Burns*, vol. 45, no 1, pp. 103-113, Feb. 2019. Available: ScienceDirect, https://www.sciencedirect.com/science/article/pii/S0305417918302596.
- [12] Wound Source. (2022). Scar Management [Online]. Available: https://www.woundsource.com/patientcondition/scar-management
- [13] American Academy of Dermatology Association. (2022). Scars: Signs and Symptoms
 [Online]. https://www.aad.org/public/diseases/a-z/scars-symptoms
- [14] C. Roques, "Pressure therapy to treat burn scars," *Wound Repair and Regeneration*, vol. 10, pp. 122-125, May 2002.
- [15] S. Chris, "The true cost of burn," *Burns*, vol. 38, no 7, pp. 967-974, Nov. 2012.Available: ScienceDirect

https://www.sciencedirect.com/science/article/pii/S030541791200174X#tb10005.

- [16] O. Rei, A. Satoshi, "Endothelial dysfunction may play a key role in keloid and hypertropic scar pathogenesis – Keloids and hypertrophic scars may be vascular disorders," *Medical Hypotheses*, vol. 96, pp. 51-60, Nov. 2016. Available: Elsevier https://www.sciencedirect.com/science/article/pii/S0306987716302766#f0020.
- S. Rathbun, A.Kirkpatrick, "Treatment of chronic venous insufficiency," *Current Treatments Options in Cardiovascular Medicine*, vol. 9, pp 115-126, May 2007.
 Available: SpringerLink https://link.springer.com/article/10.1007/s11936-007-0005-6.
- J. Black, P. Alves, C. Brindle, "Use of wound dressings to enhance prevention of pressure ulcers caused by medical devices," *International Wound Journal*, vol. 12, no. 3, pp. 322-327, Jul. 2013. Available: Wiley Online Libraries https://onlinelibrary.wiley.com/doi/full/10.1111/iwj.12111.
- [19] M. Fierheller and R. Sibbald, "A Clinical Investigation into the Relationship between Increased Periwound Skin Temperature and Local Wound Infection in Patients with Chronic Leg Ulcers," Advances in Skin & Wound Care, vol. 23, no. 8, pp. 369-379, Aug. 2010. Available: Ovid https://oce.ovid.com/article/00129334-201008000-00008/HTML.
- [20] Alps Alpine, "Force Sensor," HSFPAR003A datasheet, Jan. 2018 [Revised Mar. 2019].
- [21] Maxim, "High-Slop, Low-Power, Analog Temperature Sensor in an SC70 Package," MAX6612MXK datasheet, Jul. 2002.
- [22] Amazon. (1996-2022). Mxfans 100xGold-Plated 6mm Copper Probes Spring pogo Pin Connector [Online]. Available: https://www.amazon.com/Mxfans-Gold-plated-Copper-Needles-Connector/dp/B07FQF2BRC.
- [23] TestEquity, "Temperature Chamber," Model 105 datasheet, Feb. 2002.

82

- [24] Microchip, "High-Performance Microcontroller with XLP Technology," PIC18(L)F26K22 datasheet, 2010-2012.
- [25] Maxim Integrated, "Ultra-low Offset/Drift, Precision Instrumentation Amplifiers with Buffer," MAX4208 datasheet, May 2015.
- [26] Linear Technology, "200mA Buck-Boost Synchronous DC/DC Converters," LT3531 datasheet, Aug. 2007.
- [27] DSD TECH, "Bluetooth module," HM-10 datasheet, Jan. 2001.
- [28] MILL-MAX, "SPRING-LOADED PIN," 0965 datasheet.
- [29] Microchip, "16-Bit, Multi-Channel delta-sigma ADC with I2C Interface and On-Board Reference," MCP3426 datasheet, 2009.
- [30] DIODES, "300mA RF ULDO REGULATOR," AP2210 datasheet, Mar. 2021.
- [31] Hirose Electric Co., LTD, "Low Profile Connector," DF58 Series datasheet, Nov. 2016.
- [32] J. Skelly, "Monitored Compression Therapy: Using Smart Technology to Optimize the Treatment of Lower Extremity Swelling," M.S. thesis, Dept. of ECE, UNLV, Las Vegas, NV, 2022.

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